



Position Statement and Practice Guidance

Audiological assessment and hearing aid provision for patients with a programmable ventriculo-peritoneal (PVP) shunt

Date: March 2021

Due for review: March 2026



General foreword

This document presents Practice Guidance by the British Society of Audiology (BSA). This Practice Guidance represents, to the best knowledge of the BSA, the evidence-base and consensus on good practice, given the stated methodology and scope of the document and at the time of publication.

Although care has been taken in preparing this information, the BSA does not and cannot guarantee the interpretation and application of it. The BSA cannot be held responsible for any errors or omissions, and the BSA accepts no liability whatsoever for any loss or damage howsoever arising. This document supersedes any previous recommended procedure by the BSA and stands until superseded or withdrawn by the BSA.

Comments on this document are welcomed and should be sent to:

British Society of Audiology
Blackburn House,
Redhouse Road
Seafield,
Bathgate
EH47 7AQ
Tel: +44 (0)118 9660622

bsa@thebsa.org.uk
www.thebsa.org

Published by the British Society of Audiology

© British Society of Audiology, 2021

All rights reserved. This document may be freely reproduced for educational and not-for-profit purposes. No other reproduction is allowed without the written permission of the British Society of Audiology.





Authors

Produced by: The Electrophysiology Special Interest Group and the Professional Guidance Group

Key Authors:

John E FitzGerald	Norfolk & Norwich Universities Hospital NHS Trust
Guy Lightfoot	ERA Training & Consultancy Ltd
Siobhan Brennan	University of Manchester; Sheffield Teaching Hospitals
Verity Hill	University Hospital of Coventry
Soumit Dasgupta	Alder Hey Children's NHS Foundation Trust, Liverpool
John Day	Betsi Cadwaladr University Health Board, North Wales

Declarations of interests

- Declaration of interests by the authors: None declared

With thanks to:

Sally Wood, Public Health England

Citation

Please cite this document in the following format:

BRITISH SOCIETY OF AUDIOLOGY (2019), *Position Statement and Practice Guidance Audiological Assessment and Hearing Aid Provision for patients with a programmable ventriculoperitoneal (PVP) shunt*. [Online]. Available from: *insert web link*. [Accessed date]

Shared Decision-Making

It is implied throughout this document that the service user should be involved in shared decision-making when undertaking audiological intervention, receiving subsequent information and understanding how it will impact on the personalisation of care. Individual preferences should be taken into account and the role of the clinician is to enable a person to make a meaningful and informed choice. Audiological interventions bring a variety of information for both the clinician and the patient which can be used for counselling and decision-making regarding technology and anticipated outcomes.





Contents

1. Abbreviations	5
2. Introduction	5
2.1 Background and aims.....	5
2.2 Scope.....	6
3. What audiology procedures pose a potential risk to the operation of a PVP shunt and how can the risk be avoided?.....	6
4. Recommended action	7
4.1 Audiology assessment.....	7
4.2 Hearing Aid Fitting	8
4.3 Recommended action if a transducer with a potential to affect a PVP shunt setting has been placed near the site of the shunt.....	9
4.4 Suppliers.....	9
Appendix 1. Common manufacturers of PVP shunts.....	10
Appendix 2. Evidence from the literature that earphones and other devices affect PVP shunts	10
Appendix 3. Transducer magnetic field strengths	10
Appendix 4. Hearing aids and hearing aid ancillary devices	12
Appendix 5. Bone anchored hearing aids	12
Appendix 6. Cochlear implant magnets (on RF transmitter coils) and processors... ..	13
Appendix 7. Common symptoms with PVP shunt malfunction	13
References	14





1. Abbreviations

FDA	Food and Drug Administration (American Government Agency overseeing safety including medical devices)
G	Gauss (a measure of magnetic field strength; 1 G = 0.1mT)
mT	milli-Tesla (The SI unit of magnetic field strength)
PTA	Pure-tone audiometry
PVP Shunt	Programmable ventriculo-peritoneal Shunt
SI unit	The International System of units

2. Introduction

2.1 Background and aims

A ventriculo-peritoneal (VP) shunt is a surgically implanted device in the ventricle of the brain which can be fitted to patients of all ages as a treatment for hydrocephalus to drain excess CSF from the brain to another part of the body. There are two types of commonly used VP shunts: Programmable shunts (PVP shunts) and non-programmable shunts (non-PVP shunts). PVP shunts have a magnetically adjustable valve placed under the skin, which is often on or near the mastoid bone to allow the shunt to be adjusted by an external control magnet if required. Appendix 1 lists some common makes.

However the magnetic valve is also susceptible to other external magnetic fields and if activated inadvertently by an external magnetic field this can trigger the shunt to adjust, cause a change in intracranial pressure which in turn may lead to a life threatening situation. The magnetic field strength¹ required to adjust the valve setting varies between different types of PVP shunts. Some adjustable valves can be readjusted by relatively weak fields. An in vitro study by Zuzak et al., 2009 found the Strata valves could be readjusted by magnetic fields ranging from 0.4mT to 13.8mT with a median of 4.7mT and the Codman Hakim valves by magnetic fields ranging from 2.4mT to 153mT with a median of 30.5mT. Newer valves (Polaris, ProGAV, ProSA, and Certas) have mechanisms intended to prevent accidental readjustments, even in MRI machines (up to 3T).

Non-PVP shunts are not susceptible to this risk.

¹ The strength of a magnetic field can be measured as magnetic flux density (B), which represents the number of magnetic field lines penetrating an area (1m²) perpendicular to it. The unit of magnetic flux is the Tesla.





Manufacturers of all PVP shunts recommend caution around external magnetic fields and that all products with magnets are kept at least 5cm from the implant site. This is because magnetic field strength decreases significantly with a small change in distance. For example a decorative refrigerator door magnet may have a magnetic field strength of 100 mT at the magnet surface, but 0mT at 5cm, an iPad smart cover 206mT at its surface and 0.13mT at 5cm. This is supported by the FDA who suggest keeping products that contain magnets at least 2 inches (5.08cm) from the PVP shunt valve.

Given the above, any magnetic field generated by an audiological device or equipment that reaches the PVP shunt programming levels (when measured at 0mm distance) poses a risk.

This position statement aims to highlight the potential risks posed by audiological equipment and hearing aids to patients with PVP shunts and to provide recommendations to minimise such risks.

2.2 Scope

This document provides examples of magnetic field measurements emitted by some audiological equipment, hearing aids and hearing aid ancillary devices, collated from a number of sources available at the time of publication and highlights the potential risks posed to patients with PVP shunts. It does not set out to provide an exhaustive list for specific equipment and what is safe or not safe. Readers are advised to consult with both PVP shunt manufacturers to identify safe levels of magnetic flux for specific shunts and with audiological equipment suppliers/hearing aid companies to establish magnetic field strengths emitted by specific equipment. It is recognised that some Audiology services may undertake their own surveys of magnetic field levels for locally used equipment, typically with support of local medical physics colleagues. In such cases the Audiology services may use this local data to perform a risk assessment and determine locally appropriate mitigating measures.

3. What audiology procedures pose a potential risk to the operation of a PVP shunt and how can the risk be avoided?

Earphones, (supra-aural and circum-aural), insert earphones, ear muffs/cups, bone conductor transducers, otoacoustic emission probes, tympanometer transducers, conventional hearing aids, bone osseointegrated hearing devices and cochlear implants, all contain magnets which emit an external magnetic field (even when not in use) and their use should therefore be considered with caution when dealing with a patient with a PVP shunt. Evidence from the literature that earphones and other devices can influence PVP shunts is presented in Appendix 2.





Appendix 3 Table 1 and Table 2 give the magnetic field strengths of a range of commonly used transducers in Audiology departments. This implies that earphones, such as TDH39, TDH49 and DD45 have the potential to affect a PVP shunt if positioned directly over the site of the shunt, but do not pose a risk if kept 5cm from the shunt at all times. As this is unlikely to be possible for the testing of an ear on the side of a shunt, the use of such earphones on the side of a shunt must be considered a risk.

The B71 and B72 bone conduction transducers do not reach the median levels at which the PVP shunts referenced in this document are triggered but given some shunts were adjusted by levels as low as 0.4mT the margin of safety is small so this guidance currently adopts a cautious approach.

Eartone 3a insert earphones do not reach the levels at which the PVP shunts referenced in this document are triggered and can be used with caution. This is supported by the Speech-Language & Audiology Canada (Alberta College of Speech-Language Pathologists and Audiologists , 2015).

All conventional hearing aids emit a magnetic field, and both the specific internal components and other ancillary equipment they are used with should be considered in relation to the potential risk to alter the performance of a PVP shunt (Appendix 4, Table 5 and 6).

Pierson et al (2017) showed that for osseointegrated hearing aids (BAHA5, BAHA BP110, and Oticon Ponto Plus Power) the magnetic field strength at 5cm did not represent any risk to PVP shunt operation, but that the Sophono bone conducting hearing aid had a considerably higher magnetic field strength and additional caution was required with the Sophono (Appendix 5, Table 7).

The magnetic retention discs in the cochlear implant speech processor RF coils (Appendix 6, Table 8) have a high magnetic field strength at their surface and some at 2cm.

Where the presence of a PVP shunt restricts the ability to achieve a comprehensive audiological assessment or compromises the ability to provide optimal amplification this needs to be discussed with the patient / carer and the neurosurgical team.

4. Recommended action

4.1 Audiology assessment

Prior to audiology assessment all subjects should be asked if they have a PVP shunt and which make and model it is. If they do have a PVP shunt the following is advised unless the tester is





certain the make and model is not prone to magnetic field strengths emitted by the transducers being used;

Do not place the following transducers on or near the ear with the PVP shunt valve;

- Supra-aural or circum-aural earphones (this also includes ABR earcups)
- Bone conductors²
- Otoacoustic emission probes , except for Titan TEOAE and DPOAE systems and Otodynamics Otoport systems, see Appendix 3, Table 1 and Table 4)
- Tympanometer transducers (a cautious approach is adopted due to current lack of evidence of emitted magnetic field strengths), except for the GSI39 and Titan Tympanometers, see Appendix 3, Table 1.

Ear inserts can be used, but a cautious approach is recommended by keeping the transducer part at least 5 cm from the mastoid containing the shunt valve at all times.

Bone conduction testing can be performed on the ear contralateral to the PVP shunt valve.

Newborn hearing screening should only be performed using equipment which has been demonstrated to be safe through nationally recognised magnetic field measurements. In the absence of that and until that time, babies with a PVP shunt should not undergo newborn hearing screening and should be referred directly to the local Audiology service for ABR testing using inserts.

Children with a PVP shunt should not undergo school hearing screening with earphones and should be referred directly to the local Audiology service for testing using inserts.

4.2 Hearing aid fitting

Services should seek manufacturers' advice regarding the magnetic field strengths emitted by the range of hearing aids they prescribe, with particular attention to hearing aid ancillary equipment, such as magnetic switch activators.

Prior to hearing aid fitting all subjects should be asked if they have a PVP shunt. If they do the following is advised;

² For adult PTA the bone conductor can be placed on the forehead, as long as this is 5cm from the mastoid with the PVP shunt and correction factors applied as defined in BS EN ISO 389-3, Table C.1. For newborn ABR diagnostic testing the forehead placement is not recommended as there are no known correction values for a forehead bone conduction placement and the effect on threshold determination is unknown.





- Consult with the specific shunt manufacturer (or the patients' neurosurgery department) and hearing aid manufacturer to identify the safe level of magnetic field strength and to establish the potential risk.
- If the magnetic field strength emitted by the device is within the safe level for the PVP shunt in question continue with the fitting if required on the side of the PVP shunt, otherwise explore options to re-locate the hearing aid where viable to avoid a hearing aid fitting (conventional, osseointegrated or cochlear implant) to the side with the shunt.
- Do not implant a Sophono osseointegrated hearing aid on the side of a PVP shunt (Appendix 5, Table 7).
- If a decision is taken to proceed with an osseointegrated hearing aid or cochlear implant on the same side as a PVP shunt, the osseointegrated hearing aid, or in the case of a cochlear implant, the transmitter coil magnet and internal magnet should be at least 5 cm from the shunt valve.

For existing hearing aid users with a PVP shunt where no previous consideration has been given regarding the risk to altering the shunt setting the same advice as above should be followed.

4.3 Recommended action if a transducer with a potential to affect a PVP shunt setting has been placed near the site of the shunt.

Inform the patient or carer that there is a possibility that the shunt settings may have been affected by placing the transducer/hearing aid near the shunt. They will be familiar with the symptoms of shunt malfunction to look out for (see appendix 7) and if they experience any symptoms they should be advised to see their neurosurgical team immediately. Contact the neurosurgical team as soon as the error is realized and follow their advice.

If there is uncertainty about which type of shunt a patient has, a cautious approach should be adopted and the advice regarding PVP shunts should be followed.

If an adverse reaction is identified local risk management procedures should be followed which may include reporting the incident to the National Patient Safety Alert Committee.

4.4 Suppliers

Manufacturers of audiological equipment, including hearing aids and associated worn equipment, should routinely provide information on magnetic field strengths at set distances from the device. This requirement should also feature in procurement of equipment by services and agencies.





Appendix 1. Common manufacturers of PVP shunts

Codman-Hakim and the Codman Certas™ programable valve (Codman Integra)
 Strata adjustable valve (Medtronic Neurologic Technologies)
 Polaris adjustable valve (Sophysa)
 Miethke proGAV (Aesculap Inc)
 Sophy adjustable valve (Sophysa)

Appendix 2. Evidence from the literature that earphones and other devices affect PVP shunts

In *in vitro* experiments, Spader et al (2015) demonstrated that Apple earbuds, Beats by Dr. Dre, and Bose QuietComfort Acoustic Noise Cancelling earphones all reprogrammed the Strata™ II and Codman-Hakim PVP shunts at 0mm to the shunt valve when the earphones were rotated 180° on the valve. The Bose earphones reprogrammed the valves when brought into contact with them. However above a distance of 5cm none showed magnetic field strengths above the manufacturers' recommended levels (Appendix 3, Table 3). Zuzak et al (2009) demonstrated that magnetic toys could alter the settings on Strata and Codman valves.

A case report of a Programmable Strata™ II valve being maladjusted by a hands-free wireless communication device worn by a nurse in a hospital environment when it was inadvertently brought close to a baby's head demonstrates the potential dangers of external magnetic fields influencing programmable shunt valves (Fujimura et al 2018).

Appendix 3. Transducer magnetic field strengths

Table 1. Magnetic field strength measurements from audiology equipment transducers (personal communication with Dr Guy Lightfoot (November 2018, and July 2019), John Day (July 2019) and Sune Thorning Kristensen*, Johannes Callø* and Jens Fritze** (April 2020).

Transducer	Range of Magnetic Field Strength (mT) at			
	0mm	5mm	20mm	50mm
TDH39 Ear Phone from front grill or rear	19 - 27	8 – 15	1.1 – 2.5	0.14 – 1.0
B71 Bone conductor side/back/top	0.3 - 5			
B71 Bone Conductor - face plate (circular contact area at front)	1.1 – 1.7	0.5 – 0.9	0 – 0.2	<0.1
B81 Cone Conductor – side	15.5			
- circular contact plate	5.7			
DD45 Supra-aural earphone - front grill	28			
- rear	14			





DD45 S Supra-aural earphone - front grill	13			
Eartone 3a and IP30 Insert earphone	<0.1			
Hand held warbler (Soundfield) Interacoustics PA5	1.3	1.3	0.7	0.20
NBHS earphone Algo 3i (various placements on transducer)	<0.1			
GSI 39 Tympanometer Probe	<0.1			
Titan Clinical probe (New)	<0.1			
Titan Clinical probe (old)	<0.1			
DD450	1.8			
DD65v2a	1.8			

*Technical Product Managers, Interacoustics. **Compliance Supervisor, Interacoustics.



Figure 1. Placement of magnetic field probe over body of Eartone 3a insert.

Table 2. Magnetic field strength measurements from Obata et al. (2016)

Transducer	Magnetic Field Strength (mT)
TDH49P Ear Phone at Front Grill	25.3
B72 Bone Conductor circular contact area at front	7.4

Table 3. Measurements from Spader et al (2015)

Transducer	Magnetic Field Strength (mT) at 0mm	Magnetic Field Strength (mT) at 5mm	Magnetic Field Strength (mT) at 50mm
Apple earbuds	19.6	5.1	0
Beast by Dr Dre	26.7	14	0





Bose QuietComfort	24	13.4	0
-------------------	----	------	---

Table 4. Magnetic field strength measurements from Otodynamics (2018)

Transducer	Magnetic Field Strength (mT) at 0mm
Otodynamics Otoport probe (OAE & ABR)	≤0.1

Appendix 4. Hearing aids and hearing aid ancillary devices

Table 5. Measurements from personal communication with John Day (July 2019)

Hearing Aid	Magnetic Field Strength (mT) at device surface
Starkey Contact Mini BC (on face plate)	1.7 – 2.0
Phonak Sky Q70-M13	<0.1
ReSound Danalogic CS91 (Max O/P Full Loop system)	<0.1
ReSound Danalogic UP967 (Max O/P Full Loop system)	<0.1

Table 6. Measurements from personal communication with Jordi Cornado, Technical Support Audiologist, Phonak, UK. (September 2018).

Transducer	Magnetic Field Strength (mT) at 0mm direct on disc surface (middle of disc)	Magnetic Field Strength (mT) at 3mm (in direction of the cylinder axis)
Phonak EasyPhone magnet disc (SAP No 054-0024; Magnet Reed Switch Activator for Auto T-Coil)	315	110

Induction measured with magnet field probe Mk IV, Maurer Magnetics

Appendix 5. Bone anchored hearing aids

Table 7. Measurements from Pierson et al. (2017)

Transducer	Max Magnetic Field Strength (mT)	Magnetic Field Strength (mT) At 5mm	Magnetic Field Strength (mT) At 50mm
Cochlear BAHA5	0.11		0
Cochlear BP110	3.62		0
Oticon Ponto Plus Power	4.87		0
Medtronic Sophono	>80	3.48	

Conclusion Safe to use as long as valve is ≥ 5mm from the magnetic attachment.





Appendix 6. Cochlear implant magnets (on RF transmitter coils) and processors

Table 8. Measurements from personal communication with John Day (July 2019)

Cochlear Implant Device measured face to skin	Magnetic Field Strength (mT)	Magnetic Field Strength (mT) At 20mm	Magnetic Field Strength (mT) At 120mm
Cochlear System 7 Magnet: Half M	18		<0.1
4iM	42		
Cochlear System 6 Magnet: Half M	80		<0.1
5M	370		
Cochlear System 5 Magnet: Half M	85		
5M	340	8	0.05
Medel Rondo Magnet 6M	340	8	0.05
Cochlear System 6 Processor	0.1		
Medel Rondo Processor	0.1		

(120 mm = approximate distance across head in an infant)

Appendix 7. Common symptoms with PVP shunt malfunction

- Vomiting with little or no nausea
- A constant, unrelieved headache
- Vision problems, such as blurry, double vision, or loss of vision
- Irritability
- Fatigue
- Personality changes (not acting like your normal self)
- Loss of coordination or balance
- Swelling, redness, or both, along the shunt path
- A bulging soft spot on an infant's head
- Difficulty waking up or staying awake
- Decrease in school performance





References

- Alberta College of Speech-Language Pathologists and Audiologists (June, 2015)
Attention SLPs and Audiologists working with clients with programmable implanted medical devices (cardiac and VP shunts). Speech-Language & Audiology Canada
- BS EN ISO 389-3: Acoustics. Reference Zero for the Calibration of Audiometric Equipment. Part 3: Reference Equivalent Threshold Sound Pressure Levels for Pure Tones and Bone Vibrators. (Identical to ISO 389-3)
- Dasgupta S (March 2018) Cheshire-Mersey group protocol – hearing assessment and amplification options in programmable intracranial shunts
- FDA (1/5/18) Magnetic Field Interference with Adjustable CSF Shunts.
<https://www.fda.gov/medical-devices/cerebral-spinal-fluid-csf-shunt-systems/magnetic-field-interference-adjustable-csf-shunts>
- Fujimura, R., Lober, R., Kamian, K., Kleiner, L. (2018) Maladjustment of programmable ventricular shunt valves by inadvertent exposure to a common hospital device. *Surg Neurol Int* 9:51
- Obata, S., Ujihashi, Y., Munekata, S., Ishii, N., Kanoh, Y. (2016) Influence of hearing inspection using headphones and a bone conduction vibrator on a programmable valve shunt system. *Kitasato Med J* 46: 8 – 14.
- Pierson, MJ. (2017) Programmable shunt valve interactions with osseointegrated hearing devices. *J Neurosurg Pediatr.* Apr;19(4):384-390
- Spader, HS., Ratanaprasatporn, L., Morrison, JF., Grossberg, JA., Cosgrove, GR. (2015). Programmable shunts and headphones: Are they safe together? *J Neurosurg Pediatr.* 16:402–405
- Zuzak, TJ., Balmer, B., Schmidig, D., Boltshauser, E., Grotzer, MA. (2009). Magnetic toys: forbidden for pediatric patients with certain programmable shunt valves?. *Childs Nerv Syst* 25:161–164

